

WO 2005/008238

PCT/FR2004/001810

**METHOD AND DEVICE FOR THE ANALYSIS OF LIVING REACTION
MEDIA**

5 The present invention relates to a method and a device for the analysis of reaction media comprising one or more cells, this method and this device making it possible to perform an automated high-throughput analysis.

10 Currently, in biological research, and in particular in the pharmaceutical field, attempts have been made to analyze the phenotype of cell populations, and more particularly the proteome, in response to one or more stimulations exerted on these cell populations, so as
15 to evaluate the impact of these stimulations on the cells to which they are applied. This analysis requires tools for carrying out reactions on living reaction media (cell populations) and the analysis of these reaction media under conditions such that there is no
20 (or as little as possible) distortion of the reaction medium between these two steps, so as to limit the loss or transformation of the information.

25 There exists, in this research field, an increasing demand in terms of sample processing throughput. An increasing number of molecules are available to be tested, and increasingly varied cell systems (tissues, networks, cells) are available to be studied.

30 There exists therefore a need for tools for analyzing living reaction media, which make it possible to study these reaction media with as much objectivity as possible and with a processing rate that is as high as possible.

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The present invention, which allies the culturing of cell populations on matrix supports and analysis by

mass spectrometry, makes it possible to satisfy these expectations.

At the current time, phenotypic screening is carried
5 out essentially using colorimetric methods, or
fluorescent or radioactive molecules. These methods
require the labeling of specific molecules, which means
that the protein(s) investigated must be known
beforehand. The present invention does not require any
10 prior knowledge of the expected modifications of the
cells subsequent to the stimuli.

Many methods today make it possible to analyze more or
less directly the phenotype of one or more cells with a
15 more or less rapid throughput.

The analyses directly using cells all have an operating
principle in common, but differ with respect to the
signal analyzed at output, which represents the
20 phenotype:

- optical signal: fluorescence, luminescence,
colorimetry.
- radioactive signal: labeled molecules.
- electrical signal: electrophysiology.

25 These various analytical methods are generally
implemented in a plastic well format (96 or 384 wells
per plate) which also requires a large amount of
reagents (0.1 to 0.5 ml per well in a 96-well plate)
30 and allows only a moderate throughput.

In addition, the signal is not directly representative
of the phenotype, but requires a calibration that is
often complex.

35 It is, moreover, difficult to directly analyze cell
secretions, except by means of antibody uptake methods.

Analysis of the various phenotypes is done only on the basis of a single parameter, a molecule that is known, and for which the intention is to verify whether it is present or not: it is necessary, at the start, to know
5 which molecule is being sought. For example, when the intention is to study the presence of a molecule in the cell, it is necessary, at the start, to have quite a precise idea of the various properties of this molecule, so as to couple it to a specific antibody or
10 render the molecule fluorescent. It is also possible to look for post-translational modifications of proteins, but by targeting a specific modification.

Research relating to the limit of the performance and
15 processing rate of these various methods has led to the development of a format that is more suited to very high-throughput handling. The first example of the result of this research is DNA chips: the messenger RNAs expressed by a cell population (after stimulation)
20 are screened in the form of deposits on a matrix support, or chip, containing DNA fragments potentially complementary to this expression. This method makes it possible to assess the level of expression of several thousand genes on a chip.

25 However, the results are often not demonstrative enough to be able to do without a finer study after a first analysis. In fact, this method involves sample processing steps (collection and multiplication of the
30 amount of RNA, reverse PCR) that move away from the cellular model under consideration. In addition, it only makes it possible to analyze the level of expression of RNA, which is not directly related to the amount of proteins produced, nor to the qualities
35 thereof, due in particular to post-translational modifications (alternative splicing, modified quaternary 3D conformation, phosphorylation, assembly).

Other molecule chips attempt to overcome this distancing by trying to directly analyze the level of expression of various molecules within the cell culture. Thus, various molecules have been deposited in the form of a matrix on supports in the chip format: RNA, proteins, sugars, for example. Unfortunately, the techniques used are not really reliable, and are intended to analyze interactions between molecules rather than a cell phenotype.

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Finally, even though the number of different molecules analyzed on a chip is large, a choice has already been made with regard to the molecules that are deposited onto the support. This approach implies prior knowledge of the phenotypes being sought, which restricts the analytical possibilities.

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As regards cell chips, they have been described by Sabatini et al. These cell chips function in the following way: DNA is deposited in the form of a dispersion in gelatin, as a matrix, on a glass slide. After drying, the positions comprising DNA are treated with a lipid based transfection agent and the plate is then placed in a medium into which cells are dispensed. On the glass slide, the gelatinized DNA is present in solid form and the transfection takes place in a semi-solid phase, by binding the molecules adjacent to the DNA deposits to lipids that promote penetration of the DNA into the cells adjacent to the DNA deposits. A matrix of transfected cells at the positions corresponding to the DNA deposits is obtained. This method has the drawback of not being very precise and of being nonreproducible. The attachment by the gelatin does not make it possible to control the detachment of the transfected DNA. Neither does it make it possible to improve the transfection efficiency. Using this method, the expression or the blocking of the expression of a sufficient amount of protein is difficult to obtain. Only one type of cell can be used

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for each glass slide. It is not possible, by this means, to study the interaction between cells or the interaction between cells and reagents other than DNA.

5 Compared with the analytical methods listed above, mass spectrometry constitutes a tool that is much more advantageous in terms of the relationship between the signal detected and the cell phenotype (the molecules expressed by the cell and their respective amounts). It
10 in fact makes it possible to directly measure the amount of proteins present in a sample, without it being necessary to modify the integrity of the molecule (by labeling of the molecule, for example). The principle consists in desorbing from a solid support
15 and ionizing molecules of the sample to be analyzed. Then, the mass/charge ratio of the particles thus created is recorded; it represents the signature of the desorbed molecule.

20 In the use currently made thereof in cell biology and in proteomics, many sample treatments are necessary (cell lysis, sample purification, introduction of a matrix for MALDI spectrometry, for example), because the specificity and the accuracy allowed for the moment
25 by the instrumentation does not permit a direct analysis of the samples, the quality of which is not controlled to a high enough degree. These treatments introduce biases into the analysis, which is no longer really representative of the cell phenotype.

30 In addition, the implementation of these methods and the use of the existing equipment allows only a very low sample treatment throughput.

35 A new system (**SELDI** for "surface enhanced laser desorption ionization") for using mass spectrometry on more or less complex samples that is a little closer to the cell model, has recently been developed. The asset of this system comes from its ability to perform some

of the purifications necessary for obtaining a correct analysis, directly on the support which goes into the machine (selective and oriented adsorption at the surface of the support), which makes it possible to shorten and simplify the sample treatments.

This system is used in particular in the discovery of a disease marker: samples from a sick population are analyzed with respect to others from a normal population, and the differences are analyzed by means of a proprietary program; this makes it possible to identify markers for the disease, and therefore potentially advantageous targets. This method makes it possible to perform really an overall analysis of the samples: the molecules that will be the markers for the disease are not known beforehand.

However, sample treatments are still necessary (cell lysis, washing and purification) in order to obtain good results. For example, the cells are cultured away from the substrate, which implies a non-controlled sample transfer bias. Moreover, the analytical throughput is still low: the chips that can be used in this system can contain only 16 different plots to date.

Several documents concerning mass spectrometry relate to the analysis of living reaction media:

- Document US-2002/0160420 describes the analysis by mass spectrometry of a sample of human serum that has undergone several purification steps.

- Document US-2002/0076739 describes a method for analyzing proteins in mixtures. Labeled reagents specific for certain peptides are reacted with protein mixtures, and the molecules that have reacted are isolated and then analyzed by mass spectrometry.

- Document DE 10038684 describes a method for identifying microorganisms using a MALDI-TOF-MS system, in which the spectrum of a sample of a microorganism to be identified is compared with a database of reference spectra.

- Document US-6,531,318 describes a method for analyzing biological tissues, this method comprising a step consisting of microdissection by means of a laser, this microdissection making it possible to select cell aggregates, followed by mass spectrometry analysis.

- Document WO 00/48004 describes a device for analyzing cellular material. Cells are cultured, purified by methods other than chromatography, and then injected into a mass spectrometer.

This method requires handling of the cell culture samples; in particular, the purification is a step in the method which eliminates certain constituents of the sample, without the selection of the components that are eliminated being completely controlled.

- Document WO 02/103360 describes a method for analyzing proteins at the surface of a cell; this method comprises reacting the cell with a substance at its surface and analyzing it by mass spectrometry.

- Document WO 01/65254 describes a method for identifying the chemical structure of a substance present in tissues or cells of various organisms, this method comprising the irradiation of a precise area of a section of living tissue or of a cell, so as to ionize the substance and determine its mass spectrum, and the analysis of this spectrum so as to identify its structure.

- Document WO 02/101356 describes a method for analyzing mitochondrial proteins. The proteins

constituting the mitochondrion are separated by two-dimensional gel electrophoresis and then analyzed by mass spectrometry.

5 - Document WO 01/84143 describes a method for analyzing a large number of proteins in a small amount of time. Cells are subjected to a stimulation and lyzed, and the samples are divided up so as to obtain batches of a few hundred proteins, and these batches
10 are then analyzed by mass spectrometry using a battery of spectrometers in parallel.

The methods for analyzing living reaction media by mass spectrometry all comprise one or more purification
15 and/or handling steps that result in a loss of information, and/or they imply the search for well-defined molecules, whereas one of the objectives of the invention was that of obtaining an analysis without any constraints regarding the data expressed by the living
20 reaction medium.

In addition, these methods of the prior art, because of the purification and/or handling steps that they comprise, are not very suitable for high-throughput
25 treatment.

By comparison with the techniques of the prior art, the method and the device of the invention have many advantages:

30 - possibility of working on an assortment of varied cells arranged on the same chip,
 - varied cell systems placed in parallel,
 - elimination or limitation of steps liable to bias the analysis (such as purification, cell lysis,
35 movement of a sample from one medium to another),
 - possibility of analyzing a very large number of samples in a small amount of time,
 - obtaining of data not distorted with respect to the information emitted by the cell.

A subject of the invention is therefore a method for analyzing at least one reaction medium comprising at least one cell C, said method being characterized in that:

(i) the cell C is deposited onto a support S comprising a substantially planar surface, in the form of an aqueous drop on said surface;

(ii) the substantially planar surface of the support S onto which the aqueous drop containing the cell C has been deposited is optionally covered with a separating film F that allows gases to pass through and prevents evaporation of the aqueous drops deposited onto the support S;

(iii) the cell C is optionally subjected to a stimulation;

(iv) the reaction medium is prepared and introduced into the mass spectrometer;

(v) the reaction medium is desorbed and ionized;

(vi) the mass spectrum of the reaction medium is recorded and analyzed.

A subject of the invention is also a device for analyzing at least one reaction medium comprising at least one cell C, this device being characterized in that it comprises:

- a support S comprising a substantially planar surface optionally covered with a separating film F that allows gases to pass through and prevents evaporation of the aqueous drops deposited onto the support S,

- means for depositing onto said surface, and optionally under the film F, aqueous drops containing the cell C,

- means for desorbing and ionizing the reaction medium,

- a mass spectrometer.

The device of the invention may also optionally comprise a controlled-atmosphere chamber in which the support S is placed so as to allow the survival of the cell C.

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The stimulation to which the cell C is subjected may vary in nature. It may consist of:

- the introduction of a reagent R,
- being brought into contact with one or more
10 cells,
- a supply of energy,
- the application of an electric field or of a magnetic field,
- a stimulation by optical treatment.

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Several variants exist for the introduction of a reagent R into the cell C:

• According to a first variant, an aqueous drop
20 containing the cell C is deposited onto the support S, and a second aqueous drop containing the reagent R is injected, using any suitable injection means, directly into the drop containing the cell C. Such a variant is illustrated in Figure 1.

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• According to a second variant, a first aqueous drop is deposited onto the support S and then a second aqueous drop is deposited onto the same support in proximity to the first; one of these drops contains the
30 cell C, the other the reagent R, and the reaction of the reagent R with the cell C and, optionally, its transfection into the cell C is triggered by the fusion of the two drops. The displacement and the fusion of these drops can be obtained by vibration within the
35 support, by electrophoretic displacement of the electrically charged drops or by means of mechanical or optical clamps. It can also be obtained by a modification of the surface properties of the support, brought about by the application of an electric or

magnetic field, or by a suitable thermal or optical treatment. Such a variant is illustrated in Figure 2.

According to a third variant, the reagent R is
5 attached to the support S or to the film F, the cell C
is deposited in the form of an aqueous drop onto the
support S and the reagent R is then detached from the
support S or from the film F in order to allow it to
10 react with the cell and, optionally, to be transfected
into the cell. This variant is illustrated in Figures 3
and 7.

In the present invention, the term "transfection" is
used to denote the penetration of a molecule of a
15 reagent, whatever it may be, into a cell.

When the stimulation of the reaction medium comprises
the introduction of a molecule of a reagent R, the
separating film F, when it is present, is chosen so as
20 to be non-miscible with R.

Among the means for supplying energy, mention may in
particular be made of thermal treatment means, which
may consist, for example, of a heating device that can
25 be placed in proximity to the support S or attached to
this support and that is intended to bring the droplets
to an appropriate temperature. For example, the heating
means may consist of electrically conducting wires that
also serve as a means of receiving the drops.

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The optical treatment means are in particular means for
treatment with ultraviolet rays, the latter being known
to induce crosslinking between complementary strands of
DNA and between DNA and proteins.

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The bringing into contact with one or more other cells
consists in introducing one or more other cells into
the reaction medium so as to constitute a network of
cells capable of interacting.

• According to a first variant, an aqueous drop containing the cell C is deposited onto the support S, and a second aqueous drop containing one or more other
5 cells is injected, using any suitable injection means, directly into the drop containing the cell C. The order of deposition of the drops of cells can of course be reversed.

10 • According to a second variant, a first aqueous drop is deposited onto the support S and then a second aqueous drop is deposited onto the same support in proximity to the first; one of these drops contains the cell C, the other drop containing one or more other
15 cells, and the interaction between the cells is triggered by the fusion of the two drops. The displacement and the fusion of the drops can be obtained by vibration within the support, by electrophoretic displacement of the electrically
20 charged drops or by means of mechanical or optical clamps. It can also be obtained by modification of the surface properties of the support, brought about by the application of an electric field, of a magnetic field, of a thermal treatment or of an optical treatment.

25 Preferably, the support S consists of a plate that can be made of silicon, of glass or of a polymer, for instance of polyurethane, nylon, polyester, polyethylene, polypropylene, polyfluorocarbon,
30 poly(methyl methacrylate) (PMMA), polycarbonate, polyvinyl chloride (PVC), polydimethylsiloxane (PDMS) or polysulfone.

According to the invention, the attachment of the drops
35 to the support occurs due to surface tension forces. Preferably, the support S has a substantially planar surface comprising at least one means for receiving the aqueous drops.

Preferably, the means for receiving the aqueous drops consists of areas of the substantially planar surface of the support S that range from $5 \mu\text{m}^2$ to 5mm^2 in size.

5 According to a first variant, it may be envisioned that the support S exhibits a hydrophobic nature on its planar surface and comprises one or more hydrophilic areas constituting said receiving means. According to another variant, it can also be envisioned that the support S comprises, on its planar surface, cavities that range from 1 micron to 1 millimeter in depth and constitute said receiving means. It can also be envisioned that the support S is a plate that has outgrowths of small thickness, from 1 micron to 15 1 millimeter, arranged on its surface and intended to promote the attachment of the drops. Finally, it can be envisioned that the support S is a plate that has at least one wire onto which the drops attach. The depositing of two drops onto the same receiving means 20 will promote the fusion of these two drops and therefore the reaction of the reagent R with the cell C. Preferably, the support S exhibits a hydrophobic nature on its planar surface and comprises one or more hydrophilic areas constituting the receiving means. In 25 order to confer a hydrophobic nature on the planar surface of the support, said surface is preferably covered with a hydrophobic substance such as a polyfluorocarbon, for instance polytetrafluoroethylene or Teflon®, or a silane, for instance perfluorosilane. 30 The hydrophobic area of the support can consist of a surface structuring that is indented on a nanometric scale, such as the "black silicon" used in optics. Examples of commercial slides of this type are the superteflon 40-well D2 mm immunofluorescence slides 35 sold by the company Merck Eurolab division Polylabo. Even more preferably, the support also comprises a second means for receiving the drops, superimposed on the first, such as, for example, a hydrophobic planar surface and hydrophilic outgrowths of small thickness,

or a hydrophobic planar surface and hydrophilic wells, as illustrated in Figure 6, or a hydrophobic planar surface and a hydrophilic wire.

5 The support may be adapted from a support used conventionally for mass spectrometry; it may be envisioned that it comprises a layer that may be electrically conducting (steel, for example) or not; that it is covered, at least on the receiving means,
10 with a substance that promotes desorption. Such supports exist on the market, for example:

- the SELDI chips ("ProteinChip[®] arrays") sold by the company Ciphergen Inc. (model NP20, for example)
15 comprise a thin hydrophobic layer pierced with holes where the surface is active (hydrophilic);

- the "AnchorChip[™]" supports sold by the company BrukerDaltonics Inc. comprise hydrophobic surfaces on
20 which hydrophilic outgrowths are placed.

The supports may also be active, so as to cause the drops on its surface to change, using the principles of droplet microfluidics. This amounts to dynamically
25 modifying the surface properties of the support (for example, variations in surface tension/energy) so as to cause the drops to move in a controlled manner. Thus, the drops of cell cultures can go through various reaction steps carried out within the support: it is
30 possible to fuse two drops which are close together (one with the reagent and another with the cells, for example).

To produce this type of support, Shenderov *et al.*
35 ("*Electrowetting-based actuation of liquid droplets for microfluidic applications*", Applied Physics Letters, vol. 77, No. 11, p. 1725-1726, September 2000) describes the use of the modification of the surface energies of a hydrophobic layer when an electric field

is applied: the surface tension decreases with the strength of the field, the surface becomes less hydrophobic, or even hydrophilic. The control and the movement of the electric field makes it possible to
5 displace the drops of liquid on this surface. This method was patented by the company Nanolytics (Shenderov et al. "Actuators for microfluidics without moving parts", No. US 6,565,727; 2003), but without the use of cell cultures.

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Another manner in which these surface properties can be modified consists of the physicochemical modification of the surface layer of the support, still using an electric potential. For example, the change in
15 conformation of an SAM layer ("self-assembled monolayer", for example modified thiols, comprising at least one hydrophilic end and one hydrophobic chain), demonstrated by Lahann et al. ("*A reversibly switching surface*", Science, Vol. 299, p. 371-374, January 2003),
20 makes it possible to go from a straight conformation of the molecules within the surface layer, which then is hydrophilic in nature, to a curved conformation, in which it is hydrophobic in nature.

25 Similarly, the temperature can be used as a means of changing the surface properties of a support. Liang et al. ("*Preparation of Composite-Crosslinked Poly (N-Isopropylacrylamide) Gel Layer and Characteristics of Reverse Hydrophilic-Hydrophobic Surface*" Journal of
30 Applied Polymer Science 72:1, 1999) describes a polymer which is hydrophilic at low temperatures (< 30°C) and hydrophobic above this. By integrating a system of localized control of the temperature under the substrate, it is possible to control the surface
35 properties.

It is also possible to set up a support for which the properties of the surface layer change according to whether or not light is applied (electromagnetic

field). Ichimura et al. ("Light-driven motion of liquids on a photoresponsive surface", Science, Vol. 288, p. 1624-1626, June 2000) describes such a surface: a layer of polymer (calyx[4] resorcinarene),
5 the terminal group of which (azobenzene) can change isomeric conformation after asymmetric photoirradiation. When these cyclic groups in the *trans* conformation (hydrophilic layer) are exposed to UV radiation (365 nm), they change to the *cis* conformation
10 (hydrophobic). The reaction is reversible using blue light (436 nm). By selectively and gradually lighting the polymer layer, it is possible to displace liquid drops in a controlled manner.

15 According to a variant of the invention, the reagent R is attached to the support S before depositing of the aqueous drop containing the cell C. Such devices are known to those skilled in the art for other uses: they are the DNA chips as described by:

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- Eisen M.B., Spellmann P.T., Brown P.O., Botstein D. Cluster analysis and display of genome-wide expression patterns, *Proc Natl Acad Sci USA*. 1998 Dec. 8; **95**(25); 14863-8;
 - 25 - Haab B.B., Dunham M.J., Brown P.O., Protein microarrays for highly parallel detecting and quantitation of specific proteins and antibodies in complex solutions, *Genome Biol*. 2001 Jan 22; **2**(2): RESEARCH 0004.1-0004.13;
 - 30 - Livache T., Bazin H., Caillat P., Roget A., Electroconducting polymers for the construction of DNA or peptide arrays on silicon chips, *Biosens Bioelectron*. 1998 Sep 15; **13**(6): 629-34.

35 The same principle can be applied to molecules other than polynucleotides. Molecule chips are described in: Kuruvilla et al., Glucose signalling with small molecule microarrays, *Nature* (2002), 416 p. 653. In all

cases, the reagent molecule is first attached to the chip (for example by covalent attachment to a glass slide). According to the present invention, the molecule may optionally be detached after depositing of
5 the aqueous drops containing cells onto the molecule chip.

The detachment of the reagent molecule can be carried out in a known manner by one of the following means:

- 10 - UV-photocleavage using a site for binding of the reagent to the support which is photocleavable, as illustrated in Figure 5.

In addition, when the reagent is a polynucleotide only:

- 15 - cleavage of the double-stranded DNA with restriction enzymes, or with other nucleases,
- modification of the hybridization stringency: a change in salt concentration, in temperature or in redox conditions of the medium makes it possible to
20 separate two DNA strands.

In certain cases, it is envisioned that the reagent R remains attached to the substrate.

25 According to the invention, the substantially planar surface of the support S may be covered with a separating film which performs three functions:

- it must prevent unwanted fusion of the aqueous drops,
30 - it prevents evaporation of the aqueous drops deposited onto the support,
- it allows gases to pass through, in particular O₂ and CO₂, the latter two functions being intended to allow the cells to survive in their drops.

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The film F may be varied in nature:

- it may be a non-water-miscible liquid such as, for example, an oil. Up until now, it was known how to use oil to preserve certain cells; however, it had never

been used to carry out reactions on cells. Among the oils that can be used in the method and the device according to the invention, mention may in particular be made of mineral oils and silicone oils. It is also
5 possible to use, as liquid, an organic solvent that is non-miscible with the compounds to be treated (cells and reagents), such as, for example, octane. A light mineral oil is preferably used;

- it may also be a gas such as air saturated with
10 moisture;

- it may subsequently be a flexible, solid film, such as a PDMS (polydimethylsiloxane) film or a nitrocellulose film;

- finally, it may be a rigid honeycombed cover made
15 of porous material, the size of the cavities being adjusted so as to be able to contain the drop of cell(s) and, optionally of reagent. According to a variant of the invention, the rigid honeycombed cover may be functionalized, in each cavity, with a reagent
20 molecule and may thus constitute a molecule chip or a nucleotide chip destined to come into contact with the support onto which drops of cells have been deposited in a manner that is symmetric with respect to the cavities. This variant of the invention is illustrated
25 in Figure 7.

Before introduction of the reaction medium to be analyzed into the mass spectrometer, the separating film, if it is liable to impair the implementation of
30 the steps of this analysis, is removed.

When there is no separating film or when the latter is a gas or a liquid, the aqueous drops containing a cell or a reagent are advantageously deposited onto the
35 support S, and optionally under the separating film, by means of fine capillaries, as illustrated in Figure 1. Preferably, these capillaries are connected to a pump or syringe pump making it possible to control the volume of the drops.

The cells and the reagents can also be dispensed by means of a conventional system such as those used for the fabrication of DNA chips. Mention may, for example, be made of piezoelectric systems for compressing a cavity and ejecting a drop via a nozzle. Reference may be made, on this subject, to N. Takada *et al.*, Proceeding of the SID, Vol. 27/1, **1986**, 31-35.

Preferably, the ejected drops pass through the liquid or gas film by virtue of their rate of ejection and/or by gravity, this liquid or this gas being lighter than the solution to be deposited. When the separating film is a solid film or a rigid cover, it is deposited onto the support, after depositing of the aqueous drops of cells and, optionally, of reagents, by the same means as described above.

The displacement and the fusion of the drops can be obtained by vibration within the support, by electrophoretic or electromagnetic displacement of the electrically charged drops or by means of mechanical or optical clamps. It can also be obtained by modification of the surface properties of the support, brought about by the application of an electric field or of a magnetic field, by thermal treatment or optical treatment, etc.

Preferably, the support S of the device is mobile, so as to allow it to move from a first depositing means to a second depositing means, and optionally to other depositing means, and also so as to allow it to move to the mass spectrometer. The support S may, in certain cases, consist of a solid film attached to rollers at its two ends, the rollers being equipped with winding means so as to allow displacement of the film and therefore displacement of the drops which have been deposited on it.

Generally, the method according to the invention envisions the displacement of the support S after the depositing onto the support S of the first series of drops, regardless of whether they are drops of cells or drops of reagent.

According to the invention, the support S may be placed in a controlled-atmosphere chamber, the temperature, the hygrometry and the CO₂ content of which are adjusted so as to allow the cells to survive.

Such devices are in particular controlled-atmosphere incubators. The temperature in such a device can range from 35 to 42°C, a preferred temperature being between 36.5 and 37.5°C. Temperature variation may in particular be used to induce cell differentiation.

The CO₂ level is preferably maintained at between 3 and 5%. The oxygen O₂ level is preferably that of ambient air.

For example, it is possible to envision maintaining the cells in aqueous drops on the support S in an incubator at 37°C, with 95% air, 5% CO₂ and 97% humidity.

It is generally envisioned that only the supports onto which have been deposited the drops of cells and the separating film are placed in a controlled-atmosphere chamber. However, other elements of the device of the invention can, if necessary, be placed in this chamber.

Advantageously, it is possible to envision that the aqueous drops containing one or more cells, a cell tissue or a cell network comprise a culture medium.

In fact, the establishment of cell cultures depends on the ability of the cells to maintain their proliferation and therefore on the conditions essential to their growth.

Advantageously, it is envisioned that the aqueous drops of cells comprise MEM, or minimal essential medium, sold by Gibco BRL under the Cat. reference
5 No. 12000-022.

The culture medium may also contain other constituents, such as calf serum, one or more antibiotics intended to control the sterility of the medium, for instance
10 penicillin.

It is also possible to envision using, in the culture medium, chemical agents which induce cell differentiation, for instance bromodeoxyuridine.
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It is also possible to envision that the aqueous drops in which the cells C are cultured are gelled, using any known gelling agent, for instance agar or gelatin.

Advantageously, the aqueous drops containing the cell(s) or the cell tissue or the cell network, and/or the aqueous drops containing the reagent, comprise one or more constituents intended to promote transfection, for instance liposomes. Such transfection agents are
20 described in particular in documents WO 01/20015 and
25 WO 98/33932.

Other means intended to promote transfection can also be used in the device of the invention, such as:
30 electroporation or microprecipitation. These transfection methods, which are well known to those skilled in the art, are described in particular on <http://opbs.okstate.edu/~melcher/MG/MGW4/MG43.html>.

It can also be envisioned that the device comprises means of detection focused on one or more drops deposited onto the support.
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The means of detection are in particular devices intended to measure the fluorescence or the radioactivity of one or more drops or of the cells contained in one or more drops.

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The means used in the devices according to the invention will preferably be connected to a control device making it possible to automate the device and the method according to the invention.

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The use of the device and/or of the method according to the invention has many advantages: very small amounts of materials can be used: a single cell per drop makes it possible to carry out a transfection experiment and
15 is sufficient to perform a mass spectrometry analysis. It is possible to work with very small drop volumes, of less than 1 microliter, preferably of 0.1 to 1000 nanoliters containing 1 to 500 cells, even more preferably of 0.1 to 10 nanoliters containing 1 to 10
20 cells. Advantageously, drops containing from 1 to 100 cells are used. It is also possible to envision working on larger volumes, in particular greater than a microliter (10 to 100 μ l, containing 500 to 100 000 cells). This method also makes it possible to use small
25 amounts of reagent. The separating film F makes it possible to control the gas exchanges of the culture medium of the cell and its sterility. It also makes it possible to separate drops that are not intended to react together. The cell cultures in the form of drops
30 under the separating film can be conserved for at least 24 hours and for up to several days without any notable modifications of their cellular activity being observed (without notable influence on the proliferation and growth of the cells).

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The method and the device according to the invention also make it possible to carry out batteries of reactions:

Several aqueous drops each comprising at least one cell can be deposited onto the support S, said drops being isolated from one another. Preferably, each of these drops is placed in a different receiving means. All the
5 cells may be identical, but it is also possible to envision placing different cells (at least two sorts of different cells) in the various drops. Drops containing the reagent(s) are deposited in proximity to each drop containing a cell so as to allow the fusion of one drop
10 containing the appropriate reagent with the drop containing the targeted cell. It is also possible to envision injecting a drop of reagent directly into each drop of cell. For carrying out batches of reactions, a support comprising means for receiving the drops,
15 arranged evenly in the form of matrices, is advantageously envisioned so as to allow the method to be automated.

Advantageously, the support and the capillaries
20 intended to deposit the aqueous drops of cells and of reagents are connected to control means so as to allow the method to be automated.

The method and the device according to the invention
25 therefore make it possible to carry out, simultaneously and in an automated manner, a large number of reactions of a reagent on a cell, varying the nature of the reagent and of the cell, while at the same time working on extremely small volumes, and then to analyze the
30 result of these reactions.

Among these cells that it may be advantageous to study by means of this method, mention may in particular be made of:

- 35 - primary cells,
- hybridomas,
- cell lines: the cells can perpetuate endlessly and thus form lines,

- stem cells: they are obtained from a sample taken from an animal or from biopsies,
- a piece of cell tissue (the cells are not individualized),
- 5 - mixtures of the various types of cells stated above.

The cells are cultured in (aqueous) culture medium in a known manner. It is also possible to culture
10 heterogeneous cells for several days and to use this mixture.

According to a variant of the invention, when all the cells to be reacted on the same support are identical,
15 the procedure may be carried out in the following way: the support is a hydrophobic plate comprising hydrophilic areas, it is immersed in an aqueous solution containing the cells, and then it is removed from this solution, allowing the excess liquid to run
20 off. The drops of the medium containing the cells are retained in the hydrophilic areas. This step is followed by the depositing of a layer of separating film F and by the depositing of the drops containing a reagent or other cells. Depending on the nature of the
25 film F (fluid or solid), it is deposited before or after the depositing of the drops of reagent or of other cells.

Among the reagents R that can be used in the method and
30 the device according to the invention, mention may be made of:

Chemical molecules of all natures, in particular inorganic molecules, natural organic molecules,
35 molecules derived from organic synthesis and from combinatorial synthesis, molecules extracted from biological samples, and molecules extracted from biological samples, that have been modified by synthesis. Mention may in particular be made of

polynucleotides: single-stranded and double-stranded RNA molecules, single-stranded and double-stranded DNA molecules; PNA (peptide nucleic acid) molecules, which are peptide-nucleic acid chimeras; ribozymes; double-stranded interfering RNAs or proteins and peptides. Among the proteins, mention may most particularly be made of transcription factors.

The reagent molecules can be formulated in a solution ready to be deposited. They can also be prepared directly after depositing onto the support, for example by synthesis, in particular by organic synthesis, *in situ*, or by *in vitro* transcription in the drop. Prion-type molecules can also be obtained in the drop by peptide polymerase chain reaction or PCR before transfection thereof into the cells. When nucleic acid molecules are used, they can be prepared by nucleic acid PCR. As has already been disclosed above, the reagent can also be attached to the support.

When DNA is used as reagent, it is advantageously in precipitated form. Calcium phosphate can, for example, be used in a known manner. The DNA precipitation can also be carried out in the aqueous drop deposited onto the support, by fusion with a drop of the appropriate reagent.

According to a variant of the device and of the method according to the invention, it is possible to envision making several successive deposits intended to be fused:

It is possible to envision successively depositing several reagents intended to transfect the same cell, and observing their cumulative effects;

It is also possible to envision depositing several drops of cells and causing them to fuse, so as to reconstitute a cellular network of identical or

different cells in order to be as close as possible to conditions encountered *in vivo*. For example, it is possible to reconstitute networks of neurons on the scale of a few cells, by means of glial cells
5 encountering neurons, so as to make them communicate within the same drop as illustrated in Figure 4, or interactions between various types of cells which make up the skin, in order to mimic the behavior thereof on a cellular scale.

10

It is also possible to reconstitute a cellular tissue intended to mimic the behavior of the epidermis by culturing together, within the same drop, keratinocytes on a layer of collagen. It is also possible to culture
15 together skin stem cells in the presence of hair follicle cells in order to study their interactions.

For example, it is possible to use the transfection of reagents into a first type of cells in order to trigger
20 a cellular reaction, such as the production of a recombinant protein, and then to react this first cell population with a cell population of another type by fusion with another drop.

25 According to a variant of the invention illustrated in Figure 8, it is also possible to envision that the support is equipped with separating means that make it possible to separate two different cell types but that permit the passage of small molecules between these
30 cells. Such a separating means is intended to mimic a biological barrier, such as, for example, the barrier that exists between the blood and cervical cells. Such separating means are advantageously arranged on the receiving means, on the support. In order to use them,
35 it is envisioned to deposit an aqueous drop comprising at least one cell of a first type onto one side of the separating means and an aqueous drop comprising at least one cell of a second type onto the other side of the separating means. The fusion of the drops on either

side of the separating means allows communication between the cells by means of molecules capable of diffusing through the separating means. This communication can then be studied by any means, in particular by the addition of reagents in the form of an aqueous drop before or after the fusion of the cell drops. Through the automated transfection of these drops, it is possible to analyze the biological role of the factors transfected in a biological multilayer.

10

The separating means that can be used according to this variant of the invention are artificial membranes such as, for example, a nitrocellulose filter, silicon pierced with nano-holes, blotting paper, a cloth filter; the use of a solid gel, such as an agarose, collagen or gelatin gel, can also be envisioned.

15

The device and the method according to the invention make it possible to study the automated expression of recombinant proteins obtained by the entry of coding DNA into cells, to carry out the screening of nucleic acid molecules intended to modify (to block or, on the other hand, to increase) gene expression in cells, and to search for genomic promoter sequences. This invention also makes it possible to study the interactions between cells of different types, this interaction being triggered by the mixing of the drops. The device and the method according to the invention make it possible to obtain an overall view of the biological effects of the reaction of molecules of all types with cells, and in particular of the automated entry of molecules of all types into cells.

20

25

30

According to a variant of the invention, it is possible to envision one or more steps consisting in treating the reaction medium directly on the support S before its introduction into the mass spectrometer. These treatment steps can consist of a cell lysis, one or more washes, the adsorption or the attachment of

35

molecules that have an affinity for molecules whose presence it is intended to detect.

5 Next, the reaction medium placed on the support S is prepared with a view to introducing it into the mass spectrometer.

10 This preparation may consist in freezing the reaction medium so as to preserve its characteristics. It may consist in drying, with or without thermal treatment, with or without vacuum, for instance by lyophilization. It may also be envisioned to fix them by treatment with an agent such as methanol or formaldehyde. The application of several successive preparation steps may
15 be envisioned.

According to the method of the invention, when the mass spectrometer is of the MALDI type, the preparation of the reaction medium with a view to introducing it into
20 the mass spectrometer comprises, in a known manner, the addition of one or more acid molecules that are small in size and absorb light, for instance alpha-cyano-4-hydroxycinnamic acid, nicotinic acid or sinapinic acid. Said molecule in solution is added to the reaction
25 medium to be analyzed such that, after drying, the sample to be analyzed is included in the crystalline matrix formed by this molecule, which makes it possible to ensure successful desorption and ionization of the sample.

30 The solution of molecule intended to form the crystalline matrix is advantageously added to the reaction medium in very large molar excess so as to promote the formation of the crystalline matrix during
35 the air-drying of the entire mixture. When another type of spectrometer is employed, other molecules that promote desorption are used, in a manner known to those skilled in the art.

The reaction medium is then desorbed and ionized. This step is carried out with a means of desorption selected from: a laser beam, a beam of ions, a beam of neutral atoms, a beam of electrons. The desorption/ionization
5 can also be carried out by spraying of a liquid sample. The resolution is of the order of the size of the beam and allows very precise targeting of the reaction medium that it is desired to desorb. When a plurality of reaction media are on the support S, each of the
10 deposits can be targeted, and therefore desorbed/ionized, successively.

Each of the reaction media deposited onto the support S is desorbed and ionized individually and its mass
15 spectrum is also produced in an individual and targeted manner.

The support S is placed in the mass spectrometer and each of the reaction media placed on this support is
20 treated individually. The same reaction medium can be treated several times (several thousand laser treatments) so as to give a more complete analysis of the phenotype under consideration.

25 The arrangement of the deposits on the support S in the form of a matrix allows the desorption and ionization to be automated.

- Mention may be made of the following known systems
30 as means of desorption/ionization:

- o MALDI: matrix assisted laser desorption ionization and its counterpart of the
- o SELDI: surface enhanced laser desorption ionization
- 35 o SIMS: secondary ion mass spectrometry
- o SNMS: secondary neutral mass spectrometry
- o ESI: electrospray ionization
- o FAB: fast atom bombardment
- o APCI: atmospheric pressure chemical ionization.

- Mention may be made of the following known systems as means of measuring mass:

- o TOF: time of flight,
- 5 o MS/MS: tandem mass spectrometry or multidimensional MS for MS/MS/MS/etc.,
- o quadrupole (or ion trap),
- o FT-MS or FT-ICR: Fourier-Transform mass spectrometry - ion cyclotron resonance.

10

Any combination of these various means comprising at least one means of desorption and one means of analysis can be considered according to the present invention as a mass spectrometer.

15

The mass spectrum obtained for each reaction medium can be compared with a database of mass spectra so as to allow the identification of known molecules within the reaction medium.

20

The comparison of the mass spectrum of a cell culture with that of a reaction medium derived from this culture makes it possible to identify modifications that have been involved in the cell culture subsequent to the stimulation that was applied to it.

25

The change over time in the response of a cell or of a set of cells to a given stimulation can be studied by means of the method and the device of the invention: the same stimulation can in fact be applied at intervals over time to a series of identical reaction media placed in series on the same support S.

30

The method and the device of the invention make it possible to perform mass spectrometry imaging: the molecules present in the sample are desorbed/ionized selectively on an area that is small in size (less than 100 μm - of the order of the size of the beam used), sequentially over the entire surface of the sample. For

35

each "point" of the surface a spectrum is then obtained which describes the relative abundance (concentration) of molecules present in this point of the sample. The abundance of a molecule is represented by the height of a peak (or the area of the curve under this peak) within the spectrum obtained. If one peak is selected in all the spectra, it is possible to envision recreating an "image" of the sample relative to this molecule, in the same way as for a fluorescence scanner: a point is represented, for example, by a pixel of color, associated with a color code which makes it possible to evaluate the abundance of the molecule described by the peak selected at this point; the set of pixels gives a readily interpretable image. This variant of the invention is illustrated in Figure 10.

This process can be implemented for each of the peaks present in the spectra, and therefore, from a single scan of the surface by the beam, it is possible to recreate an image of the sample for each molecule of interest detected in the sample. An analysis by fluorescence scanner generally only makes it possible to visualize molecules labeled prior to the scanning, in a sequential manner (one labeling for one molecule and for one scan).

It is also possible to select several peaks for the entire sample, each represented by a color, which is more or less intense according to the abundance of the molecule. The superposition of the two colors gives an image of the ratio of concentration of the substances with respect to one another.

The method and the device of the invention make it possible to perform the overall analysis of a sample:

The cell cultures are prepared for their introduction into the spectrometer (drying, cryogenic treatment,

addition of a matrix for promoting desorption/ionization, for example). The sample is scanned overall by the beam. A large number of spectra are recorded, which are added to give a mean of the
5 abundance of the various substances in the sample.

The method and the device of the invention make it possible to perform the overall analysis of a simplified sample:

10

In order to facilitate the analysis of the spectrum obtained during overall scanning of the surface, it is possible to simplify the sample, directly on the chip, before it is introduced into the spectrometer, using
15 active surfaces. These surfaces can make it possible to more or less specifically retain certain substances of the sample, subsequent to washing as illustrated in Figure 9.

20 The method and the device of the invention make it possible to study the change in a living reaction medium under the effect of a stimulation. This approach does not require the modifications (protein expression, for example) engendered by this stimulation to be known
25 beforehand, as is the case for the other methods for analyzing reaction media in a matrix. In addition, all the reactions that occur take place in the living cell, in the presence of the same influencing factors as in an *in vivo* test. Finally, the manipulations and
30 treatment consisting of purification and/or of extraction and/or of transfer of the reaction medium can be avoided with the method of the invention, which makes it possible to avoid the artifacts and the biased observations that are specific to *in vitro* study
35 systems.

More specifically, the device of the invention comprises at least one piece of equipment for measuring the mass of a sample by means of mass spectrometry,

said piece of equipment comprising a spectrometer tube,
a device for creating a vacuum in said tube, electrical
means for applying an electrical acceleration potential
in the tube so as to accelerate the molecules of the
5 sample to be analyzed, a means for detecting the mass
of the ions formed, a means of introducing the support
S into the tube so as to allow the introduction of the
reaction media associated with molecules for promoting
desorption in the spectrometer, and a means for the
10 desorption and the ionization of some of the molecules
of this sample.

Said means for desorption and ionization is connected
to a data acquisition system so as to allow the
15 sequenced treatment of a plurality of samples to be
analyzed, placed on a support S in the form of a matrix
or chip.

The method of the invention comprises the following
20 steps:

- treatment of the living reaction medium or media
placed on the support S with a means that promotes
desorption so as to produce samples ready to be
analyzed;
- 25 - introduction of the samples (reaction media)
placed on the support S into the mass spectrometer
tube; application of a vacuum and of an electric field
in the spectrometer introduction tube so as to form an
acceleration potential; application of a
30 desorption/ionization treatment, in a controlled and
sequenced manner, to the sample(s); detection of the
mass of the ions formed; optionally, comparison of the
data recorded with a mass spectrum bank.

35 The method and the device of the invention have many
advantages:

This technology in fact makes it possible to realize thousands of independent experimental conditions on a miniature format.

5 The microdrop format allows a vigorous control of the culture conditions of the cell model throughout the various processes implemented. This control is strengthened by the integration of all the sample treatments directly on the chip, possibly by means of
10 surface chemistry: culture, stimulation, purification (optionally).

So as not to compromise this control, as for all the existing methods, no sample transfer is carried out
15 between the culturing steps and the recording of the final signal.

This recording takes advantage of the accuracy and the specificity of mass spectrometry. The latter also makes
20 it possible to analyze a sample in a multiparametric manner (several molecules analyzed in a single experiment, or even an entire proteome of interest) so as to be able to take an interest in systems without prejudging their properties.

25 This invention, by keeping the samples as close as possible to the cell culture, allows much more rapid analysis of recorded data: thousands of multiparametric experiments on a single chip. This is added to an
30 interpretation, in phenotypic terms, that is much more evident and reliable. For example, no bias is introduced with regard to the quantification of the presence of a protein (no labeling, for example).

35 In addition, by directly integrating the mass spectrometry analysis on the chip or array containing the cells, the invention takes advantage of the high resolution of the device and allows high-throughput

localized phenotype analyses (expression mapping and cell imaging).

5 These analyses are also quantitative, and therefore make it possible to study the modulation of expression over time.

10 This analytical quality applies to all the molecules present in the cell sample: secreted molecules, molecules present inside the cell (interfacing with a secretion device can also be envisioned), structural molecule.

15 Since the chemistry of the molecule only plays a role in terms of the practical implementation of the spectrometry, it is possible to detect any type of molecules produced by the cells: lipids, proteins, peptides, modified proteins, sugars, circulating RNAs.

20 The direct phenotyping of stimulated cells on a chip applies to all fields that involve the characterization of cell responses:

• Biological research: clinical and fundamental
25 research on cells and intracellular or intercellular mechanisms of functioning are greatly accelerated by the use of a tool that directly employs cells and allows a high-throughput analysis coupled with high precision.

30

• Pharmaceutical research: by testing the activity
of novel (therapeutic, toxic) molecules on living cells rapidly and in a multiparametric manner, the method of the invention makes it possible to accelerate the
35 screening process, by carrying out tests that are close to *in vivo* conditions much earlier. In addition, the search for novel targets of therapeutic interest is also accelerated since their relevance is evaluated in

a complete and relatively undisturbed cellular environment.

- 5 • Toxicology/biosensors: rapid analysis of the response of cells to toxins with respect to multiple parameters (several cell models on the same chip, for example) for, for example, the military industry or the environment industry.
- 10 • Studies of genetic manipulations of plant or animal cells.

EXPERIMENTAL SECTION

15 **Example 1: Analysis of T lymphocyte secretions: cytokine IL-2**

Advantage: Characterization of samples from patients suffering from various viruses (hepatitis C, HIV, for example) or cancers. The cytokine analyzed (IL-2) is a
20 promoter of T lymphocyte proliferation; it can be used as a therapy for strengthening the immune system. The measurement of the amount of cytokine is an indicator of the progression of the disease and/or of the therapy.

25 The principle of this experiment is to try to detect, by mass spectrometry, the secretion/production of cytokine IL-2 by stimulating T lymphocytes (DO10.11 line, property of INSERM U548). The stimulation can be
30 carried out either directly (addition of the stimulating antigen to the solution) or by means of associated antigen-presenting B lymphocytes (themselves stimulated for presentation).

35 A drop of T lymphocyte cell culture (1500 cells in a drop of 4 μ l of RPMI medium + 10% FCS_fetal calf serum + 1% PS) is deposited onto a MALDI-TOF spectrometry chip. As controls, drops containing antigen alone in solution, cytokine alone in solution, culture medium

alone, or nonstimulated cells in culture, are deposited in the same manner. Cytokine production is subsequently stimulated in the drops in question.

- 5 The matrix (saturated solution of sinapinic acid or of alpha-cyano-4-hydroxycinnamic acid) is added to each spot and dried. The chip is placed in the spectrometer and the spectra are recorded and analyzed.
- 10 Several variants can be envisioned and combined:
- the matrix is deposited before the cells,
 - functionalization of the surface using anti-cytokine antibodies, before the deposits are made, and the cells are possibly lysed after stimulation,
 - 15 - no matrix is deposited.

Example 2: Analysis of a molecular signature

The aim of this experiment is to demonstrate that it is possible to analyze a cell culture on a chip format, and more particularly to distinguish a molecular signature.

20

As a sample, we used a cell culture (jurkat line, concentration of 2×10^6 cell/ml in their culture medium RPMI + 10% FCS - fetal calf serum), and also a sample of a recombinant protein (IL-2 available from R&D Systems under the reference 202-IL-050).

25

30 The chip used is part of the ProteinChip® system sold by the company CIPHERGEN Inc., using SELDI. It is a slide covered with a hydrophobic layer pierced with hydrophilic holes, where the active surface is made of silica, having the commercial reference NP20, which makes it possible to selectively retain proteins that are hydrophilic in nature. This chip contains 8 spots marked A to H.

35

The intention was to study the spectral signature of the protein without cells on a first chip. For this, a specific dilution of the protein, ranging from 5000 U/ml for spot A to 1 U/ml for spot H (encoding
5 2500, 1000, 500, 100, 50 and 10) was placed on each spot.

Preparation of the matrix:

10 o The matrix sold by CIPHERGEN (commercial reference "EAM SPA"), sinapinic acid, is dissolved in 75 µl of acetonitrile and 75 µl of 1% TFA.

15 o The solution is vortexed for 5 min.

o The solution is centrifuged for 2 min at 10 000 rpm.

Calibration of the device:

20

o A mixture of 1 µl of "All-in-one peptide mix" and 1 µl of matrix is deposited onto a spot of the chip.

25 o This is allowed to dry in ambient air.

o The calibration procedure of the ProteinChip® program is followed.

Preparation of the chip:

30

o the slide is preincubated with distilled water (5 µl per spot for 1 min),

35 o the spots are dried using absorbent paper (without touching the surface),

o 5 µl of sample are deposited per spot,

o this is left to dry in the open air,

o rinsing is carried out with distilled water
(liquid is taken from the edge of the spot with a
pipette, several times),

5

o the spots are allowed to dry,

o the matrix for promoting desorption/ionization
(0.8 μ l) is added,

10

o it is allowed to dry,

o the step consisting in adding
desorption/ionization matrix followed by drying is
repeated.

15

Reading the chip: use of the SELDI system of the CHU
[University Hospital Teaching Center] in Grenoble
(inserm U318).

20

Settings: Intensity:	210
High mass	100 000 Da
Deflector	auto (10 000 Da)
Sensitivity	10
Optimization range:	10 000 - 20 000 Da
Center mass:	15 400 Da

25

The spectra are determined using the ProteinChip®
Software.

30

In a second step, a chip containing the samples of
interest as explained in the table below is prepared:

Spot	Sample
A	Calibration (1 μ l "All-in-one peptide mix" + matrix)
B	5 μ l of culture medium without cells (RPMI = 10% FCS)
C	5 μ l of IL2 at ... U/ml in culture medium
D	5 μ l of cells in their culture medium (concentration ... cell/ml)
E	5 μ l of cells in their culture medium (concentration ... cell/ml) (duplicate of D)
F	Idem D + 1 μ l of IL2 at ... U/ml
G	Duplicate of F
H	

The samples (B to G) are deposited onto the chip according to the above protocol.

5 **Example 3: Imaging of part of the proteom of cells (3T3 fibroblast) after UV-irradiation**

Objectives: In order to very rapidly determine the effects of a drug on the response of skin cells to UV-irradiation, and to aid with the targeting of these
10 drugs to a specific cellular compartment, it is advantageous to study the distribution of some of the proteins expressed by these cells.

15 **Implementation:**

Cells (3T3 fibroblast) are cultured in a drop on a stainless steel MALDI target (for example, available from Brüker Daltonics Inc.). Drops of culture media
20 without cells are deposited onto the chip in the same manner, as controls. The chip is placed in a controlled-atmosphere and controlled-temperature chamber (37°C, 100%, H₂O, 5% CO₂).

25 Several chips are thus fabricated.

The chip is incubated for 24 h so as to allow the cells to adhere.

5 The drops are subsequently irradiated selectively through an appropriate mask, that allows the UV radiation to pass only onto the spots supposed to receive it, with several irradiation times (by changing the masks during the experiment) and/or several
10 intensities (mask more or less opaque).

After stimulation, the cells are left in culture for several incubation times (one chip per incubation time), for example, 0, 1 h, 4 h, 24 h and 48 h, so as
15 to analyze the change in phenotype.

The samples are then frozen, matrix is added thereto (sinapinic acid, for example) and they are dried and then introduced into the mass spectrometer so as to be
20 analyzed therein.

A mean of 50 spectra (equivalent to 50 laser bursts) per point (or pixel) is recorded, one point having a resolution of the size of the laser beam (less than
25 25 μm in diameter). For each point, the spectrum gives us a set of peaks. A suitable program makes it possible to select a peak of interest, and an image of the distribution of the compound described by this peak over the entire sample is retranscribed.

30

The mass of the compounds of interest allows us to refer back to its nature (by consulting databases), or else, if it is an unknown compound, the experiment can be repeated while adding more complete analysis thereto
35 (for example, by following the first spectra with a multidimensional MS analysis).

Example 4: Imaging of the distribution of calcium ions in cell cultures by TOF-SIMS and laser SNMS

Advantage: calcium ions tend to accumulate in damaged
5 cells.

Implementation:

The cells are cultured on a silicon chip, and are
10 subjected or not subjected to one or more mechanical stresses, and the samples are then treated cryogenically.

They are subsequently introduced into the spectrometer
15 under vacuum (beam of ions of 50 to 200 nm in diameter) and scanned with the beam under the same conditions as in Example 3.

The results are developed according to the same steps
20 as in the previous example.

Example 5: Demonstration of a spectral profile corresponding to a specific phenotype

25 The aim of this experiment is to illustrate the discrimination between several phenotypes by mass spectrometry on cell culture drops. We studied cytotoxicity phenomena with the use of CDDP (cisplatin = CIS-DIAMINEDICHLOROPLATINUM, property of INSERM unit
30 318), which is an anticancer drug used in chemotherapy; and also apoptosis (programmed cell death) with the use of TNF (tumor necrosis factor).

The chips used are part of the ProteinChip® system sold
35 by the company CIPHERGEN Inc. (see Example 2), using the SELDI system. The chip is more particularly the NP20 chip (commercial reference: C553-0043 NP20 ProteinChip Array, A-H Format), the hydrophilic surface of which is made of silica.

We used the U373 cell line (available from the supplier ECACC under the number 89081403).

- 5 All the steps that follow were carried out under sterile conditions.

Initially, the NP20 chips were immersed in 70% alcohol for 20 min and dried at ambient temperature under a
10 hood. The cell cultures (in DMEM culture medium + 10% fetal calf serum) were deposited, in 5 μ l drops, onto 2 chips as indicated in the table below:

Spot	Cells	Cytotoxicity treatments (chip No. 1)	Apoptosis treatments (chip No. 2)
A	Culture medium without cells	With CDDP (1 μ l: final concentration 5×10^{-6})	With TNF
B	20 000 cells		
C	20 000 cells		
D	20 000 cells		
E	Culture medium without cells	Without CDDP	Without TNF
F	20 000 cells		
G	20 000 cells		
H	20 000 cells		

- 15 The chips were subsequently allowed to incubate in an incubator in an atmosphere saturated with water at 37°C under 5% CO₂ for one day.

Then, in accordance with the conditions disclosed in
20 the table, 1 μ l of CDDP diluted in cell culture medium was deposited into drops A, B, C and D of chip No. 1, so as to achieve a final concentration of approximately 5×10^{-6} M. On chip No. 2, 0.2 μ l of TNF was deposited into drops A, B, C and D so as to obtain a final
25 concentration of approximately 0.01 μ g/ml.

The devices were then left to incubate as above in the incubator for 1 day.

- 5 The manipulations that follow were carried out under nonsterile conditions.

Before introduction of the chips into the mass spectrometer, they were soaked in a 2 mM Hepes
10 solution. They were allowed to dry at ambient temperature (10-15 min).

A matrix solution (sinapinic acid) was prepared beforehand according to the protocols recommended by
15 Ciphergen Inc.: the matrix was dissolved in 75 μ l of acetonitrile and 75 μ l of a 1% aqueous trifluoroacetic acid solution. The solution was subsequently mixed for 15 min on a vortex, and then centrifuged (10 000 rpm) for 2 min just before it was used.

20

2 times 0.8 μ l of matrix was added to each spot, allowing time to dry between each deposit (3-5 min).

Reading of chips:

25

The chips were then analyzed in the Ciphergen SELDI-TOF mass spectrometer.

The intention was to analyze the entire mass range
30 accessible to the spectrometer. Three analyses were therefore carried out on each chip for 3 mass ranges (low, medium and high). The spectra are produced using the ProteinChip® Software from Ciphergen Inc.

- 35 The settings were effected as explained in the table below:

Passage	Low	Medium	High
Laser intensity	178	198	230
High masses (in Da)	100 000	200 000	300 000
Deflector (in Da)	1500	3000	5000
Sensitivity	10	10	10
Optimization low masses (in Da)	2000	5000	20 000
Optimization high masses (in Da)	20 000	50 000	150 000

Laser shots were fired on positions 21 to 81 for the "low" passages, in steps of 5, with 2 heating bursts (intensity + 5) per position. They were not included in the mean of the 15 shots per position that, when added, form the final spectra. The medium passages use positions 22 to 82 and the "high" passages use positions 23 to 83.

The results of the assays are given in Figures 11, 12 and 13.

Figure 11: Example of a spectrum obtained without CDDP and without TNF. Along the x-axis is the mass to charge ratio in Daltons (Da); along the y-axis is the signal intensity (100 corresponds to saturation of the detector).

Figure 12: Representation of the differences between the spectra of the two phenotypes without TNF and with TNF.

Figure 12 shows the differences in intensity between two phenotypes for each peak of the spectra on a logarithmic scale: in blue, the profile of cells

stimulated with TNF (and therefore in apoptosis); in red, the profile of nonstimulated cells. Figure 13 shows, in the same way, in blue, the profile of the cells stimulated with TNF; in red, that of the cells
5 stimulated with CDDP; and, in green, that of the nonstimulated cells.

Figure 13: Representation of the differences between the spectra of the 3 phenotypes without either TNF or
10 CDDP, with TNF and with CDDP.

These results demonstrate that it is possible not only to differentiate between nonstimulated cells and stimulated cells, but also to differentiate between 2
15 significantly different phenotypes.

In addition, these phenotypes could not have been studied in a conventional manner before several days of incubation, the labeling being carried out after 3 days
20 for the cytotoxicity and after 6 days for the apoptosis.

The spectra obtained (see, for example, Figure 11) were subsequently analyzed in order to verify that
25 characteristic phenotype signatures were obtained.